

Polymethyl methacrylate (Linnea Safe) causes local inflammatory response after intramuscular implant in BALB/c mice but it is not observed in distant organs

Polimetilmetacrilato (Linnea Safe) provoca resposta inflamatória localizada após implante intramuscular em camundongos BALB/c, mas não é observado em órgãos a distância

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ABSTRACT

Introduction: Among its different therapeutic functions, the use of polymethyl methacrylate (PMMA) for more than a decade has stood out in the replacement of the volumes lost with the aging process and filling in wrinkles and creases. It is considered a permanent biomaterial despite its reliability is widely discussed by health professionals. **Objective:** To analyze the size of the microspheres in of three different commercialized types of PMMA, and the inflammatory process generated by the implant, as well as to evaluate possible migration of the microspheres. **Methods:** The polymers of the brands BioSSimetric[®], MetaCrill[®] and Linnea Safe[®] were analyzed by scanning electron microscope (SEM) and had the dispersion and the size of its particles determined. After this analysis, it was decided to implant in BALB/c mice the polymer of the brand Linnea Safe[®], which was the more homogeneous product. The animals submitted to polymer implantation were euthanized at 3, 7, 15, 30, 60, 90 and 120 days after implantation, allowing the weighing of the implanted paws and the histopathological analysis of some tissues. **Results:** It was observed that the implantation of Linnea Safe[®] PMMA microspheres in mice triggered an acute inflammatory process 3 to 15 days after the surgical procedure, evolving to chronic non-granulomatous inflammation with collagen deposition, tissue reorganization after 30 days of PMMA implantation up to 120 days; also, no microspheres were observed in distant organs. **Conclusion:** The Linnea Safe[®] PMMA behaved as a safe and stable biomaterial, once its microspheres were sized to prevents phagocytosis, and leads to local and controlled inflammation.

Key words: polymethyl methacrylate; foreign-body migration; inflammation; pathology.

INTRODUCTION

The polymethyl methacrylate (PMMA) was successfully synthesized for the first time in 1902. In 1994, its microspheres were linked to bovine collagen, creating a pasty vehicle easily implantable in the subcutaneous. Thereafter, a better retention was verified with the use of the collagen compounds mixed to the PMMA microspheres, evoking great and positive expectations of the researchers and the medical community. Since 1945, this acrylic resin is widely used in dentistry for the preparation of dental prostheses⁽¹⁾. This product has been increasingly used in several surgical specialties and it is known as an excellent

material for stabilization of long bones fractures⁽²⁾, craniofacial reconstructions⁽³⁾, intraocular lenses⁽⁴⁾, and filling soft tissue^(5, 6). PMMA is classified as good alloplastic material due to some of its characteristics, such as the fact that it is permanent or non-absorbable and non-degradable⁽⁷⁾. It has been extensively studied for its numerous and possible applications in the field of coatings, adhesives, sensors, optical devices, biomaterials, among others⁽⁸⁾.

In Brazil, PMMA infiltrative implants are being used to replenish the volume lost during the aging process and for wrinkles filling⁽⁹⁾, since there is evidence that it is a polymer that stimulates neocollagenesis, it causes a controlled inflammatory reaction, which stabilizes the material and sets the material in its implant

site. Delayed reactions, such as granulomas, have been observed with the use of PMMA, and are probably related to poor quality of the raw material used to manufacture the products, predisposition of each individual, collagenases, error in the implant procedure, such as variations in the size of the needle, inappropriate volume, irregular distribution and variation in the depth of the implant^(10, 11).

Several factors affect the type and intensity of the inflammatory reaction of the body tissues to the PMMA implantation for the purpose of aesthetic filling; among these, is the size of the polymer microspheres, which should be between 36–43 μm , since this seems to be the ideal size for large dermal injections, preventing phagocytosis and allowing the delivery and stabilization of this material. This size is accepted and considered by reports in the medical literature, which shows that microspheres with a diameter smaller than 20 μm trigger an inflammatory granulomatous response and are proven to be phagocytosed⁽¹²⁾, and microspheres larger than 50 μm would not be implanted effectively^(13, 14). Linked to the size of the injected microspheres, another factor that affects the stability of the implanted PMMA, and therefore, trigger the inflammatory reaction, is the amount of collagen deposition around the polymer microspheres; spheres with a diameter of 100 μm trigger the production of only 56% of fibrous connective tissue around it, while spheres with an average diameter of 40 μm promote growth of about 80% of collagen fibers. The higher the stability of the polymer, the lower the probability of dispersal and consequent exaggerated inflammatory response^(5, 6).

Lemperle, Morhenn and Charrier (2003)⁽¹⁵⁾ analyzed and compared ten products commercialized that were being used as soft tissue fillers, regarding its biocompatibility and durability. After four years of experiment, the authors were able to observe that all substances, resorbable and non-resorbable, proved to be clinically and histologically safe, even describing late, and mild, inflammatory reaction, in addition to the granulomatous reaction, the authors did not attribute such cellular changes to the implant of polymers.

Sousa *et al.* (2008)⁽¹⁶⁾ implanted PMMA (Newplastic[®]) in BALB/c mice and analyzed the presence of inflammatory response on the implantation site and the way it was manifested, in addition to evaluating the deposition of collagen. The authors concluded that intramuscular implantation of Newplastic[®] lead to collagen deposition, but did not induce a chronic inflammation, which demonstrates the biocompatibility of the material to bioplasty purposes; however it was verified the presence of mononuclear inflammatory infiltrate predominantly at the implantation site of the polymer.

Because of the scarcity of scientific articles focused on the description of specific materials in bioplasty, this study becomes

necessary once it evaluates different application materials, standardization of the size of the microspheres and possible inflammatory reaction to the implantation and whether it is possible or not to trigger adverse reactions in distant regions.

The objectives of this study is to analyze the size of the microspheres in three forms of commercialized PMMA and compare them with each other according to their homogeneity, to describe and characterize the inflammatory process generated by the implant, and to evaluate whether there is permanence of the microspheres in the implanted tissue.

MATERIALS AND METHODS

Evaluation of the size of the microspheres through scanning electron microscopy

The size analysis of the different brands of PMMA (Biossimetric[®] 30%, MetaCrill[®] 30% and Linnea Safe[®] 30%) was conducted using the scanning electron microscope (SEM) in the Microscopy Laboratory (LABMIC) in the Universidade Federal de Goiás (UFG), Goiás, Brazil.

The polymers were packaged in its commercial form (PMMA, hydroxyethylcellulose, methylparaben, propylparaben and water for injection), which was in gel inside a tube. For the analysis, it was used an aluminum sample holder, which was previously prepared by ultrasonic cleaning and drying in oven. Approximately 0.1 ml of the initial part of the sample in the tube was discarded. Then, in the clean dry tube, another part of the sample was spread using a disposable spatula to form a thin film. The tube with the PMMA sample was placed for drying in a desiccator with silica gel at room temperature for approximately 24 hours. After complete drying of the sample, it was covered with gold using a system for film deposition (Denton Vacuum, Desk V model), and analyzed in SEM, brand: Jeol, model JSM-6610.

To determine the PMMA particles-size dispersion, images were taken with fixed magnification of 200 times. The software Scandium, Olympus Soft Imaging Solutions GmbH, was used to analyze the images and determine the size of the particle, for this purpose, approximately 1,550 particles were analyzed for each brand. The same professional analyzed the three brands of PMMA repeated this methodology in a standardized procedure.

In vivo analysis

The study was conducted in female isogenic BALB/c mice aged between four and eighth weeks, bred and housed in the vivarium of

the Instituto de Patologia Tropical e Saúde Pública (IPTSP)/UFG. The 56 animals used were divided into two groups: Group 1 – 35 mice implanted with 0.1 ml (approximately 5×10^5 particles) of PMMA Linnea Safe® 30% in the gastrocnemius muscle of the left posterior limb (five animals per experimental day); Group 2 – 21 control inoculated mice with 0.1 ml saline solution (three animals per experimental day). The euthanasia was performed after 3, 7, 15, 30, 60, 90 and 120 days after the surgical procedure.

The mice were initially immobilized to allow the trichotomy in the caudal region of the left posterior limb. It was performed an orifice with a 40×12 needle puncturing the epidermis and dermis to apply 0.1 ml of PMMA Linnea Safe® 30% or saline solution by threading technique (preventing implantation in blood vessels and lymphatics vessels) with blunt micro cannula (21 G \times 25 mm) and surgical steel pistol which provided the formation of a subdermal tunneling, and intramuscular implantation of PMMA. In order to provide better distribution of the solution, a light massage was performed in the region.

Histopathological analysis

The animals were euthanized at a predetermined time by cervical dislocation. The left posterior limbs and viscera (liver, popliteal lymph nodes, spleen, kidneys and lungs) were removed and left in 4% formaldehyde. The paws were weighed and, subsequently, the gastrocnemius muscles were removed from the paws with longitudinal cuts and dehydrated in alcohol solutions of increasing concentration (80%, 90% and 100%), diaphanized in xylene and embedded in paraffin of low melting point, just like the viscera.

The blocks were cut into 5 μ m thick pieces and the slides were stained with hematoxylin and eosin (HE). All organs were processed to allow 10 serial slices of each organ in topography from the hilum, in order to evaluate the possible migration of Linnea Safe® 30% PMMA microspheres and possible inflammatory reactions caused by it in the tissue; whereas for the muscles, only a cut of the tissue was performed in the place implanted with the PMMA. The images were evaluated regarding the presence of inflammatory infiltrate and collagen deposition, in a semi-quantitatively way, by light microscopy.

RESULTS

After the morphometric analysis of the PMMA microspheres of three different brands, it was found that the majority (37.8%) of the microspheres diameter of the Biossimetric® brand (30%) is between 1-8 μ m, only 4.1% is between 36-43 μ m, and

36.7% of the diameter is larger than 50 μ m. The analysis of the Metacrill® (30%) brand showed that 76.1% of their PMMA microspheres diameter is between 1-36 μ m, 7.6% is between 36-43 μ m, and 16.3% is larger than 43 μ m. Unlike the two brands previously analyzed, Linnea Safe® (30%) presented with a more homogeneous appearance and highly concentrated microspheres, where 8% of microspheres diameter is between 1-8 μ m, 87.1% between 36-43 μ m, and only 0.3% is larger than 43 μ m (**Figure 1** and **Table**).

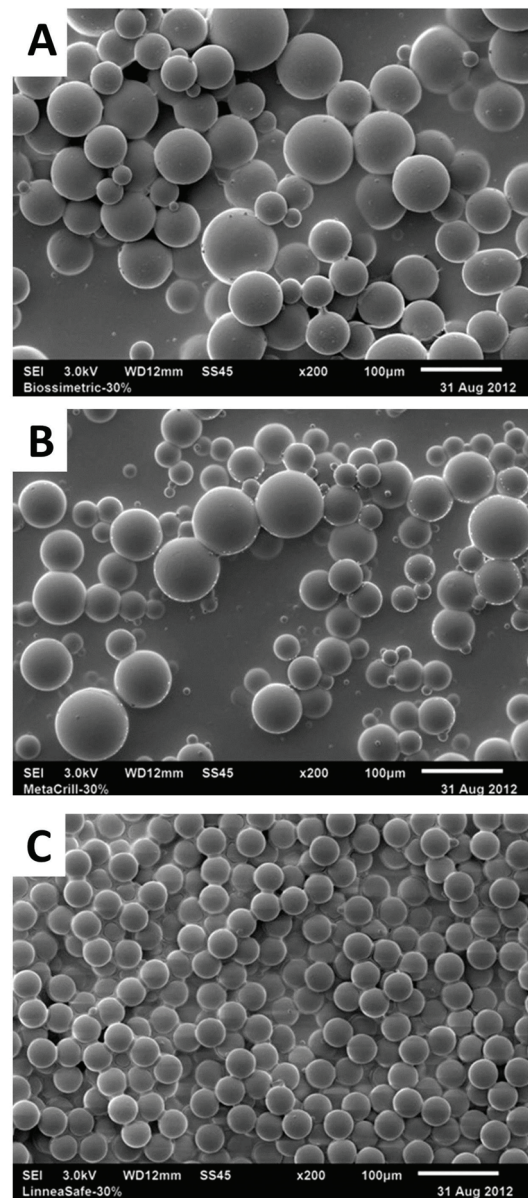


FIGURE 1 – Scanning electron microscopy of the three brands commercialized of PMMA A) Biossimetric®; B) MetaCrill®; C) Linnea Safe®, 100 μ m scale. PMMA: polymethyl methacrylate.

TABLE – Distribution of Biossimetric®, MetaCrill® and Linnea Safe® PMMA microspheres by size range using scanning electron microscopy

Size range (µm)	Biossimetric 30%		MetaCrill 30%		Linnea Safe 30%	
	Number of particles	Percentage	Number of particles	Percentage	Number of particles	Percentage
1-8	601	37.8	305	19.1	137	8.7
8-15	77	4.8	348	21.8	25	1.6
15-22	36	2.3	239	14.9	3	0.2
22-29	36	2.3	202	12.6	4	0.3
29-36	62	3.9	125	7.8	29	1.9
36-43	66	4.1	121	7.6	1,365	87.1
43-50	124	7.8	80	5	2	0.1
50-57	162	10.2	67	4.2	1	0.1
57-64	156	9.8	38	2.4	0	0
64-71	129	8.1	36	2.3	1	0.1
71-78	59	3.7	16	1	0	0
78-85	45	2.8	8	0.5	0	0
85-92	22	1.4	8	0.5	0	0
92-99	8	0.5	2	0.1	0	0
99-106	3	0.2	3	0.2	0	0
106-113	2	0.1	0	0	0	0
113-120	3	0.2	1	0.1	0	0

PMMA: polymethyl methacrylate.

The histopathological analysis of the implantation of Linnea Safe® PMMA microspheres in mice triggered an acute inflammatory process 3-15 days after the surgical procedure around the implanted spheres with the presence of important predominantly polymorphonuclear (PMN) inflammatory infiltrate, and dissociation of the muscle fibers. Between 30-120 days of the implantation of the polymer, the inflammation decreased assuming a non-granulomatous chronic profile with reorganization of the tissue with predominance of mononuclear cell infiltrates (MN) and higher deposition of collagen adhered to the microspheres and the muscle fibers. There was no necrosis, granuloma or angiogenesis in the surrounding tissue (**Figure 2**). No histopathological changes were observed in the control group.

Linnea Safe® PMMA microspheres were not found in the ten cuts of viscera (liver, popliteal lymph nodes, spleen, kidneys and lungs) in any groups throughout the analysis period. There were no PMMA microspheres in popliteal lymph nodes, but it was observed reactional aspect of this organ in the early stages of the study. There was no difference between the weights of the paws that received the implant and the other contralateral of the same animals during the study period (**Figure 3**).

DISCUSSION

The analysis of the three brands of PMMA using SEM allowed demonstrating that the Biossimetric® polymer has a greater

dispersion between the microspheres and greater variability of their size compared with the other two analyzed brands. It is considered a heterogeneous product, since spheres with a smaller diameter are more susceptible to migration and larger spheres may not be implanted correctly, preventing or hindering their fixation and better reorganization of the implanted tissue. MetaCrill® also showed significant variability in size among their microspheres, and was considered a dispersed product when spaces between the microimplants were evidenced. Unlike the brands listed and analyzed above, Linnea Safe® appeared as a homogeneous polymer, since the microspheres were concentrated, in other words, with minimal dispersion, with equal sizes, close to the expected (36-43 µm).

Piacquadio, Smith and Anderson (2008)⁽¹⁷⁾ also compared, using SEM, different PMMA commercialized brands to determine whether there are significant differences between these products, including the Metacrill, which was also analyzed in this study. Significantly morphologic differences were revealed, mainly on the size of microspheres of these polymers, leading the authors to conclude that the variability observed between these products may result in different therapeutic outcomes, especially regarding the safety of the patient. For this reason, they were able to infer that doctors and health care professionals should be aware that the products that are “comparable”, and often considered to be similar, may not be equal.

The establishment of an acute inflammatory profile on the microspheres implanted intramuscularly in female isogenic

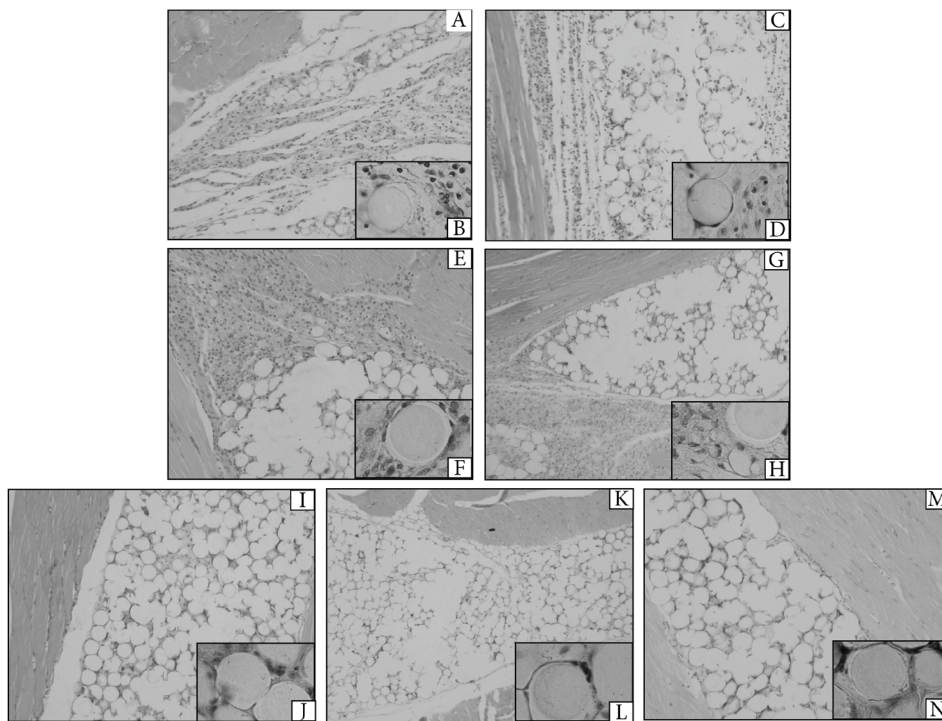


FIGURE 2 – Photomicrography, stained with HE, of the skeletal musculature of BALB/c mice after implantation of Linnea Safe®

A) damage caused by the implant in the first three days (10×, objective lens); B) increase of the previous figure highlighting inflammatory infiltrate predominantly PMN around the implanted microspheres (100×, objective lens); C) the lesion on the seventh day (10×, objective lens); D) increase of the previous figure (100×, objective lens); E) the lesion on the fifteenth day; F) increase of the previous figure (100×, objective lens); G) the lesion on the thirtieth day with decrease of the inflammatory process and the beginning reorganization of the damaged tissue (10×, objective lens); H) increase of the previous figure showing mixed inflammatory infiltrate with mononuclear cell infiltrates and collagen deposition early; I) lesion healing at the sixtieth day (10×, objective lens); J) increase of the previous figure showing greater collagen deposition, stabilization of microspheres and scarce MN inflammatory infiltrate; K) the lesion on the ninetieth day (10×, objective lens); L) increase of the previous figure (100×, objective lens); M) the lesion on the 120th day, characterized by intense collagen deposition around the implanted microspheres, discreet presence of MN inflammatory cells and complete reorganization of the damaged tissue (10×, objective lens); N) increasing of the previous figure showing stabilization of microspheres surrounded by collagen and juxtaposed.

HE: hematoxylin and eosin; PMN: polymorphonuclear; MN: mononuclear cell infiltrates.

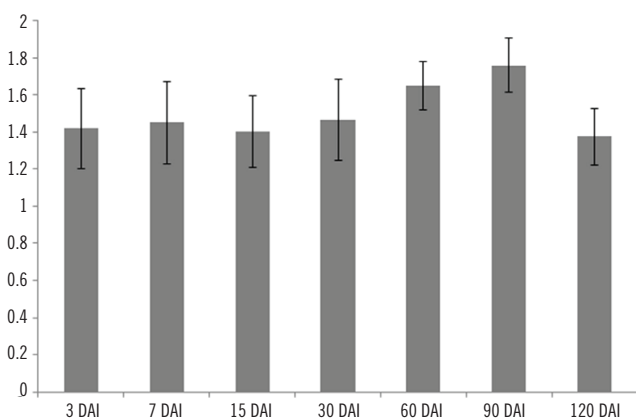


FIGURE 3 – Distribution, per experimental day, of the paws weight (in grams) of the left posterior limb of BALB/c mice after implantation of Linnea Safe®

DAI: days after implantation; $p > 0.05$ – SIGMA STAT/analysis of variance (ANOVA).

BALB/c mice is very well characterized, with a predominance of polymorphonuclear cells in the infiltrate, showing that the immune system of the animal has been activated; the infiltrate was only around the microspheres in an attempt to stop them. Around 15 days after the implantation, there was a dissociation of the muscle fibers and subsequent deposit of the host connective tissue between the microspheres, so there is a substitution of the PMMA vehicle, which is absorbable, by collagen. This finding corroborates Sousa *et al.* (2008)⁽¹⁶⁾ that described this deposition in the first month of implantation, followed by complete replacement up to three months after implantation.

After 30 days of the PMMA implantation, inflammation had a non-granulomatous chronic profile with predominance of the mononuclear cell infiltrates in the inflammatory infiltrates, reorganization of muscle tissue and enhanced collagen deposition between the implanted microspheres, similar to that Lemperle,

Morhenn and Charrier (2003)⁽¹⁵⁾ described after the analysis of the Artcoll and Jesus *et al.* (2015)⁽¹⁰⁾ when using Newplastic.

Although Morhen, Lemperle and Gallo (2002)⁽¹¹⁾ have shown that particles smaller than 20 µm are phagocytized by cells such as keratinocytes and Langerhans' cell, our study did not show that fact after the analysis of ten viscera cuts (liver, popliteal lymph nodes, spleen, kidneys and lungs) in all the groups during the period analyzed, proving that Linnea Safe[®] PMMA does not migrate, which shows that the inflammation triggered by it is local and controlled; that fact is directly related to the homogeneity of its microspheres diameter, since, as described by Lemperle *et al.*, in 2004⁽¹²⁾, the particles larger than 20 µm are encapsulated by the connective tissue, most of Linnea Safe[®]'s microspheres implanted suffer this stabilization by collagen. Despite not having found Linnea Safe[®]'s PMMA microspheres in popliteal lymph nodes,

it was observed a reactive aspect in the early stages of the study, which shows the activation of the immune system of the host when in contact with that foreign body.

It is important to highlight that the techniques most used to search for hematogenic dispersion of particles or cells is the histological analysis of the closest lymph nodes, also called, sentinel lymph node^(18,19). It is widely used in the search for metastatic cancer which allows the detection of micrometastasis in such organs⁽²⁰⁾.

Therefore, based on the analysis of this study, it can be concluded that the Linnea Safe[®] PMMA behaved as a safe and stable biomaterial, once their microspheres obey size uniformity, between 36-45 µm, preventing phagocytosis and consequent migration, which characterizes the inflammation caused by the implantation of the polymer as local and controlled.

RESUMO

Introdução: Entre suas diversas funções terapêuticas, há mais de uma década o polimetilmetacrilato (PMMA) vem se destacando na reposição de volumes perdidos com processo de envelhecimento e preenchimento de sulcos e rugas. É considerado um biomaterial permanente, apesar de sua confiabilidade ser amplamente discutida por profissionais da área da saúde. **Objetivos:** Analisar o tamanho das microesferas de três formas comercializadas de PMMA e o processo inflamatório gerado pelo implante, bem como avaliar a possível migração das microesferas. **Métodos:** Os polímeros das marcas Biossimetric[®], MetaCrill[®] e Linnea Safe[®] foram analisados por microscópio eletrônico de varredura (MEV) e tiveram a dispersão e o tamanho de suas partículas determinados. Após essa análise, decidiu-se implantar em camundongos BALB/c o polímero da marca Linnea Safe[®], o qual se apresentou mais homogêneo. Os animais submetidos ao implante do polímero foram eutanasiados aos 3, 7, 15, 30, 60, 90 e 120 dias após o implante, permitindo a realização da pesagem das patas implantadas e a análise histopatológica de alguns tecidos. **Resultados:** Observou-se que a implantação de microesferas de PMMA Linnea Safe[®] em camundongos desencadeou um processo inflamatório agudo de 3 a 15 dias após o procedimento cirúrgico, evoluindo para inflamação crônica não granulomatosa com deposição de colágeno e reorganização do tecido após 30 dias de implantação de PMMA até 120 dias; além disso, não foram observadas microesferas em órgãos a distância. **Conclusão:** O PMMA da marca Linnea Safe[®] comportou-se como um biomaterial seguro e estável, uma vez que as microesferas apresentaram tamanho que impedem sua fagocitose e provocam inflamação localizada e controlada.

Unitermos: polimetilmetacrilato; migração de corpo estranho; inflamação; patologia.

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